

A Direct D-bar Reconstruction Algorithm for Recovering a Complex Conductivity in 2-D

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Collaborators on this Project



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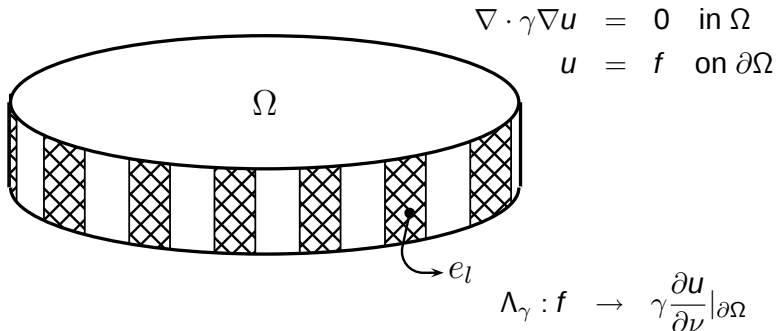
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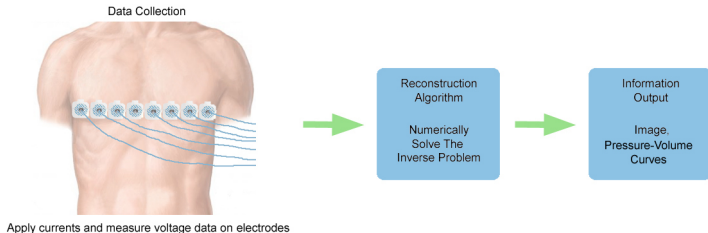
The EIT Problem

Current is applied on electrodes on the surface of the body and the resulting voltage is measured. Let $\gamma = \sigma + i\omega\epsilon$.



Mathematically, this is governed by the inverse admittivity problem: Can the admittivity γ be recovered from measurements of the Dirichlet-to-Neuman (DN) map Λ_γ ?

Applications of EIT



Medical Applications in 2-D:

- Monitoring ventilation and perfusion in ARDS patients
- Detection of pneumothorax
- Diagnosis of pulmonary edema and pulmonary embolus

Clinical Applications

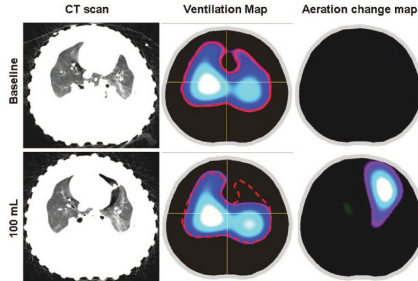


Figure 1. Computed tomography (CT), ventilation map, and aeration change map obtained at baseline (top) and after injecting 100 mL of air into the pleural space of the left upper quadrant (bottom). The arrow points to the induced pneumothorax (left, bottom).

What does the silent zone represent?

- Pneumothorax?
- Pulmonary edema?
- Hyperinflation?
- Atelectasis?

⁰Figure courtesy of M. Amato from *Real-time detection of pneumothorax using electrical impedance*

Global Uniqueness Result: Brown, Uhlmann

A classic result showed that once differentiable conductivities are uniquely determined by knowledge of the DN map Λ_σ :

Theorem

Let $\Omega \in \mathbb{R}^2$ be a bounded domain with Lipschitz boundary and σ be a measurable function bounded away from zero and infinity. If σ_1 and σ_2 are two conductivities with $\nabla \sigma_i$ in $L^p(\Omega)$, $p > 2$, and $\Lambda_{\sigma_1} = \Lambda_{\sigma_2}$, then $\sigma_1 = \sigma_2$.

Global Uniqueness Result of Francini

Assume there exist positive constants σ_0 and E such that

$$\sigma > \sigma_0 \text{ in } \Omega,$$

$$\|\sigma\|_{W^{2,\infty}(\Omega)} \leq E, \quad \|\epsilon\|_{W^{2,\infty}(\Omega)} \leq E$$

Theorem

Let Ω be an open bounded domain in $\mathbf{R}^2$ with Lipschitz boundary. Let σ_j and ϵ_j satisfy the conditions above. Then there exists a constant ω_0 such that if $\gamma_j = \sigma_j + i\omega\epsilon_j$ for $j=1,2$ and $\omega < \omega_0$ and if $\Lambda_{\gamma_1} = \Lambda_{\gamma_2}$, then $\gamma_1 = \gamma_2$.

General Overview: D-bar Methods for EIT

D-bar reconstruction methods capitalize on the direct relationship between the conductivity and CGO solutions to a PDE related to the inverse conductivity problem (possibly through a transformation).

$$\Lambda_\gamma \longrightarrow \text{Scattering transform} \longrightarrow \text{CGO solutions} \longrightarrow \gamma$$

They are

- Mesh independent
- Trivially parallelizable

General Overview: D-bar Methods for EIT

The CGO solution depends on an auxiliary variable $k \in \mathbb{C}$.

Typically, a $\bar{\partial}$ equation in z for the CGO solution leads to a direct formula for γ .

The link between the DN map and the CGO solution is through a nonlinear Fourier transform known as the **scattering transform**.

A $\bar{\partial}$ equation in the auxiliary variable k for the CGO solution involves the scattering transform and completes the constructive steps.

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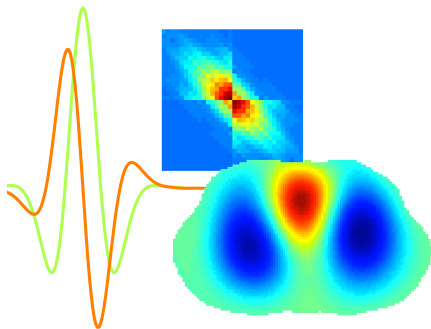
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To learn more, see our forthcoming book:

Linear and Nonlinear Inverse Problems with Practical
Applications, by JM and Samuli Siltanen

In production, SIAM 2012



The Potential Matrix

Define the matrix potential Q by

$$Q = \begin{pmatrix} 0 & -\frac{1}{2}\partial \log \gamma \\ -\frac{1}{2}\bar{\partial} \log \gamma & 0 \end{pmatrix} = \begin{pmatrix} 0 & -\frac{\partial \gamma^{1/2}}{\gamma^{1/2}} \\ -\frac{\bar{\partial} \gamma^{1/2}}{\gamma^{1/2}} & 0 \end{pmatrix}$$

and matrices D and D_k by

$$D = \begin{pmatrix} \bar{\partial} & 0 \\ 0 & \partial \end{pmatrix} \quad D_k = \begin{pmatrix} \bar{\partial} & \bar{\partial} - ik \\ \partial + ik & \partial \end{pmatrix}$$

where $\bar{\partial}_z = \frac{1}{2} \left(\frac{\partial}{\partial x} + i \frac{\partial}{\partial y} \right)$ and $\partial_z = \frac{1}{2} \left(\frac{\partial}{\partial x} - i \frac{\partial}{\partial y} \right)$.

Exponentially Growing Solutions

Given a solution $u \in H^1(\Omega)$ of $\nabla \cdot (\gamma(z)\nabla u(z)) = 0$, the vector

$$\begin{pmatrix} v \\ w \end{pmatrix} = \gamma^{1/2} \begin{pmatrix} \partial u \\ \bar{\partial} u \end{pmatrix}$$

solves

$$(D - Q) \begin{pmatrix} v \\ w \end{pmatrix} = 0 \tag{1}$$

For $k = k_1 + ik_2 \in \mathbb{C}$, seek solutions ψ of (??) of the form

$$\psi(z, k) = M(z, k) \begin{pmatrix} e^{izk} & 0 \\ 0 & e^{-i\bar{z}k} \end{pmatrix}$$

where M converges to the identity matrix as $|z| \rightarrow \infty$.

Exponentially Growing Solutions

The CGO solutions $M(z, k)$ satisfy

$$(D_k - Q)M = 0$$

Or in integral form

$$\begin{aligned} M_{11}(z, k) &= 1 + \frac{1}{\pi} \int_{\Omega} \frac{Q_{12}(\zeta) M_{21}(\zeta, k)}{z - \zeta} d\zeta \\ M_{21}(z, k) &= \frac{1}{\pi} \int_{\Omega} \frac{e_{-k}(z - \zeta) Q_{21}(\zeta) M_{11}(\zeta, k)}{\bar{z} - \bar{\zeta}} d\zeta \end{aligned}$$

and similarly for M_{12} and M_{22} , which are coupled.

Here $e_k(z) = \exp(i(zk + \bar{z}\bar{k}))$.

Computation of CGO Solutions

Applying FFT's on a suitable grid of meshsize h to the integral form of the equations

$$\begin{aligned}M_{11}(z, k) &= 1 + h^2 IFFT \left(FFT \left(\frac{1}{\pi z} \right) FFT(Q_{12}(z) M_{21}(z, k)) \right) \\M_{21}(z, k) &= h^2 IFFT \left(FFT \left(\frac{e^{-k(z - \zeta)}}{\pi z} \right) FFT(Q_{21}(z) M_{11}(z, k)) \right)\end{aligned}$$

results in a linear system that can be solved by, eg, GMRES.

Reconstruction of Q

Knowledge of the full matrix M results in a direct reconstruction formula for Q and hence γ .

Theorem

For any $\rho > 0$,

$$Q(z) = \lim_{k_0 \rightarrow \infty} \mu(B_\rho(0))^{-1} \int_{k: |k-k_0| < r} D_k M(z, k) d\mu(k).$$

This large k limit presents a problem for practical computation.

Reconstruction of Q

The following is a direct reconstruction formula for Q and hence γ involving a **small** k limit:

Theorem

Define

$$M_+(z, k) \equiv M_{11}(z, k) + e_{-k}(z)M_{12}(z, k)$$

$$M_-(z, k) \equiv M_{22}(z, k) + e_k(z)M_{21}(z, k).$$

Then

$$Q_{12}(z) = \frac{\partial_{\bar{z}} M_+(z, 0)}{M_-(z, 0)} \quad Q_{21}(z) = \frac{\partial_z M_-(z, 0)}{M_+(z, 0)}$$

The Scattering Transform

The scattering transform matrix is defined by

$$S(k) = \frac{i}{\pi} \int_{\mathbf{R}^2} \begin{pmatrix} 0 & e^{-i\bar{k}z} Q_{12}(z) \psi_{22}(z, k) \\ -e^{i\bar{k}\bar{z}} Q_{21}(z) \psi_{11}(z, k) & 0 \end{pmatrix} dz.$$

The matrix $M(z, k)$ satisfies the D-bar equation wrt k :

$$\bar{\partial}_k M(z, k) = M(z, \bar{k}) \begin{pmatrix} e_{\bar{k}}(z) & 0 \\ 0 & e_{-k}(z) \end{pmatrix} S(k),$$

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Computation

This results in two coupled systems. The first is

$$\begin{aligned}\bar{\partial}_k M_{11}(z, k) &= M_{12}(z, \bar{k}) e_{-k}(z) S_{21}(k) \\ \bar{\partial}_k M_{12}(z, k) &= M_{11}(z, \bar{k}) e_{\bar{k}}(z) S_{12}(k)\end{aligned}$$

or in integral form

$$\begin{aligned}1 &= M_{11}(z, k) - \frac{1}{\pi k} * (M_{12}(z, \bar{k}) e_{-k}(z) S_{21}(k)) \\ 0 &= M_{12}(z, k) - \frac{1}{\pi k} * (M_{11}(z, \bar{k}) e_{\bar{k}}(z) S_{12}(k))\end{aligned}$$

This can be discretized and a linear system results. Note that care must be taken with the conjugate with respect to k .

The Scattering Transform

Denote the unit outer normal to $\partial\Omega$ by $\nu = \nu_1 + i\nu_2$ and its conjugate by $\bar{\nu} = \nu_1 - i\nu_2$.

Then

$$S_{12}(k) = \frac{i}{2\pi} \int_{\partial\Omega} e^{-i\bar{k}z} \psi_{12}(z, k) \nu(z) ds(z)$$

$$S_{21}(k) = -\frac{i}{2\pi} \int_{\partial\Omega} e^{i\bar{k}\bar{z}} \psi_{21}(z, k) \overline{\nu(z)} ds(z).$$

There exist CGO solutions u_1 and u_2 to the admittivity equation with asymptotic behavior

$$u_1 \sim \frac{e^{ikz}}{ik} \quad \text{and} \quad u_2 \sim \frac{e^{-ik\bar{z}}}{-ik} \quad \text{as } |z|, |k| \rightarrow \infty.$$

and the following connection to the DN map:

$$\begin{aligned} u_1(z, k) &= \frac{e^{ikz}}{ik} - \int_{\partial\Omega} G_k(z - \zeta) (\Lambda_\gamma - \Lambda_1) u_1(\zeta, k) ds(\zeta) \\ u_2(z, k) &= \frac{e^{-ik\bar{z}}}{-ik} - \int_{\partial\Omega} G_k(z - \zeta) (\Lambda_\gamma - \Lambda_1) u_2(\bar{\zeta}, k) ds(\zeta) \end{aligned}$$

where $G_k(z)$ is the Faddeev Green's function

$$G_k(z) = \frac{e^{ikz}}{(2\pi)^2} \int_{\mathbb{R}^2} \frac{e^{iz \cdot \xi}}{\xi(\bar{\xi} + 2k)} d\xi \quad k \in \mathbb{C} \setminus 0.$$

These CGO solutions satisfy

$$\begin{pmatrix} \psi_{11} \\ \psi_{21} \end{pmatrix} = \gamma^{1/2} \begin{pmatrix} \partial_z u_1 \\ \bar{\partial}_z u_1 \end{pmatrix} \quad \text{and} \quad \begin{pmatrix} \psi_{12} \\ \psi_{22} \end{pmatrix} = \gamma^{1/2} \begin{pmatrix} \partial_z u_2 \\ \bar{\partial}_z u_2 \end{pmatrix},$$

which leads to BIE's for ψ_{12} and ψ_{21} ...

A Boundary Integral Equation for Ψ

Differentiating u_1 and u_2 leads to BIEs for the CGO solutions Ψ :

Theorem

The trace of the exponentially growing solutions $\Psi_{12}(z, k)$ and $\Psi_{21}(z, k)$ for $k \in \mathbb{C} \setminus 0$ and $\gamma = 1$ on $\partial\Omega$ can be determined by

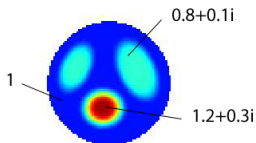
$$\Psi_{12}(z, k) = \int_{\partial\Omega} \frac{e^{i\bar{k}(z-\zeta)}}{4\pi(z-\zeta)} (\Lambda_\gamma - \Lambda_1) u_2(\zeta, k) ds(\zeta)$$

$$\Psi_{21}(z, k) = \int_{\partial\Omega} \left[\overline{\frac{e^{ik(z-\zeta)}}{4\pi(z-\zeta)}} \right] (\Lambda_\gamma - \Lambda_1) u_1(\zeta, k) ds(\zeta).$$

This provides the connection from $\Lambda_\gamma \rightarrow S$.

Steps of the Method

Given the DN map Λ_γ :



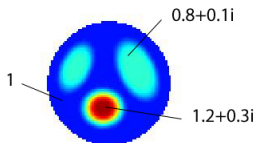
- Compute the traces of the CGO solutions u_1 and u_2 from the BIE's
- Compute the traces of the CGO solutions Ψ_{12} and Ψ_{21} from knowledge of u_1 and u_2 on $\partial\Omega$
- Compute the scattering transforms S_{12} and S_{21} from knowledge of Ψ_{12} and Ψ_{21}
- Numerically solve the system of $\bar{\partial}_k$ equations for M
- Form M_+ and M_- and compute Q_{12}
- Compute γ by solving the $\bar{\partial}$ equation

$$\bar{\partial} \log \gamma = -2Q_{21}$$

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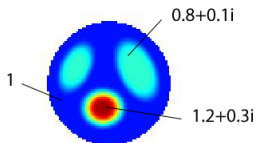


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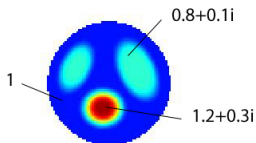


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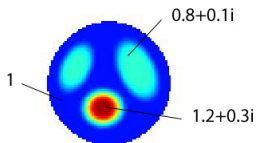


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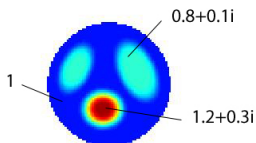


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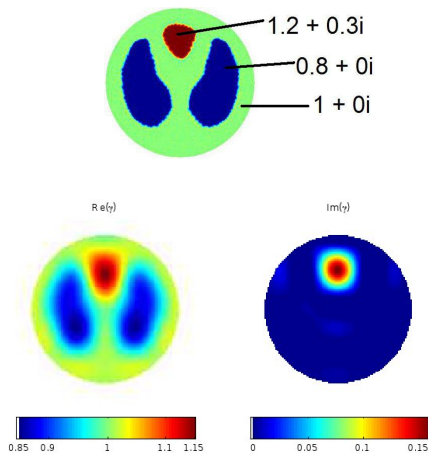
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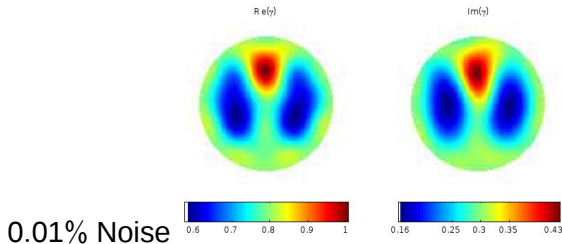
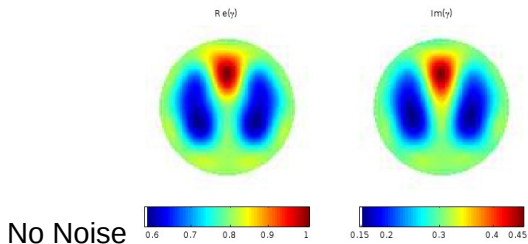
Reconstructions from Simulated Data



Dynamic range: 76% (conductivity) 53% (permittivity)

Reconstructions from Simulated Data

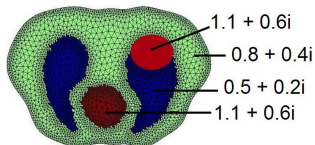
Heart: $1.1+0.6i$ Lungs: $0.5+0.2i$ Background: $0.8+0.4i$



Dynamic range: 61% (no noise) 60%, 53% (noise) ▶ ◀ ≡ ≡ ≡ ≡ ≡ ≡ ≡ ≡ ≡

Simulation of fluid in the lung

Numerical Phantom



Dynamic range

Reconstruction:

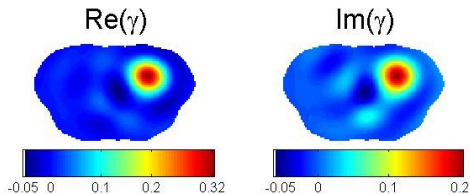
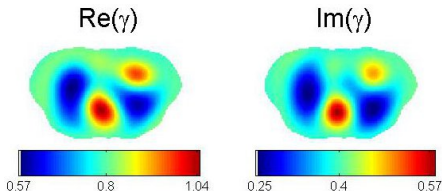
Conductivity: 80%

Permittivity: 84%

Difference image:

Conductivity: 63%

Permittivity: 67%.





**Thank you, Gunther, for all you do,
may you have many, many more Happy Birthdays!!**